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DESY, Zeuthen, Germany

25th June 2025

Status of instrumentation and new dosimetric approaches for FLASH radiotherapy



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Outline

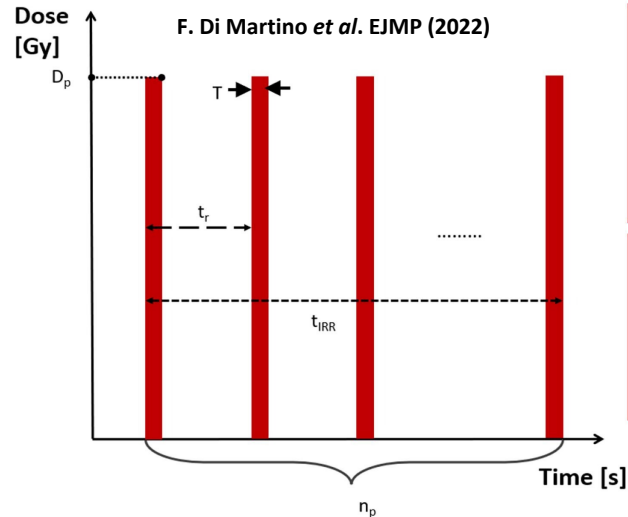
- Role of physical parameters for dosimetry of UHDR beams
- Different pulse structures and accelerators for FLASH Radiotherapy
- Limits of ionization chambers for UHDR reference dosimetry
- Adapting ion chambers and new methods to overcome limitations
- Novel approaches
- Final considerations

Involved physical parameters for FLASH radiotherapy

Physical beam parameters for conv radiotherapy:

- Particle type [e-, p, ions, X-ray, ...]
- Energy [MeV]
- Fluence [p/cm²]
- Dose [Gy]

• **Time [s]** ⚡ **FLASH (UHDR)**



T Pulse width [s]

D_p Dose per single pulse [Gy]

PRF Pulse Repetition Frequency [Hz]

n_p number of pulses

t_r time between two pulses = $1/PRF$ [s]

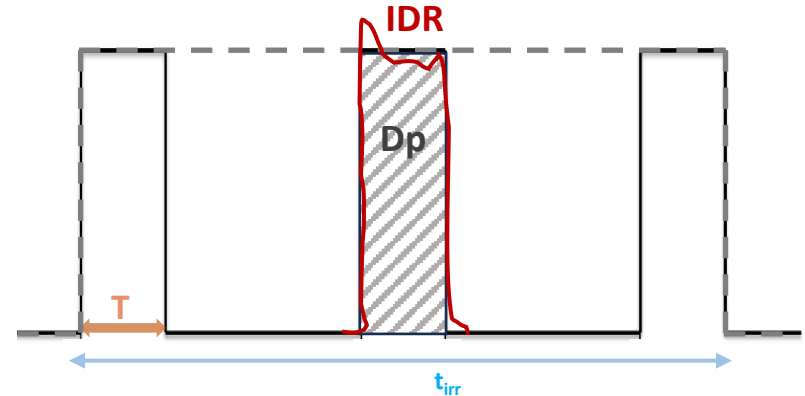
t_{IRR} total irradiation time = $\frac{n_p - 1}{PRF} + T$ [s]

DR Average dose rate [Gy/s]

$$DR = \frac{\text{Tot Dose}}{t_{IRR}} = \frac{n_p \cdot D_p}{t_{IRR}} \approx D_p \cdot PRF$$

IDR Instantaneous dose rate [Gy/s]

$$IDR = \frac{D_p}{T}$$



Requirements for ideal (active) dosimeters at UHDR:

- Linear signal-dose relationship, tissue equivalence, dose accuracy, spatial resolution, use convenience, ...
- Accurately measure the **D_p**
 - independent on DR
 - corrections to be implemented
- Accurately measure the **IDR**
- Characterize the **pulse temporal structure** (high temp. res.)
 - a combination of technologies...
- **Passive** dosimeters (alanine, RCF, Fricke):
 - Lot of work done at the beginning
 - Still used to characterize novel detectors
 - reliable, but not suitable for clinical routine

Physical parameters to look at?

CONVENTIONAL RADIOTHERAPY

Dose: ~2 Gy/fract. (x 30 fractions)

Dose Rate: ~ Gy/min

Irradiation Time: few minutes

FLASH RADIOTHERAPY

Dose: > **10 Gy** (x 1 fraction?)

Dose Rate: > **40 Gy/s**

Irradiation Time: < **200 ms**

FLASH RADIOTHERAPY

Dose = **10 Gy**

Dose Rate = **40 Gy/s**

Irradiation Time = **200 ms**

n. of pulses = **4 pulses**

$\bar{D}_0$ = **2.5 Gy**

D_p [Gy]

Average $DR_{FLASH} = 10^3 \times$ Average DR_{CONV}

IDR = **10^6** higher!

FLASH RADIOTHERAPY

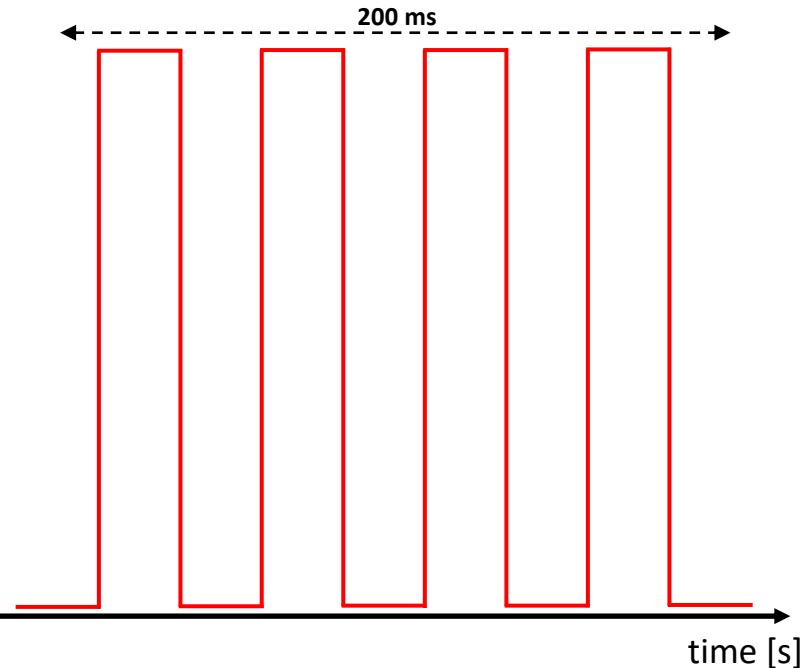
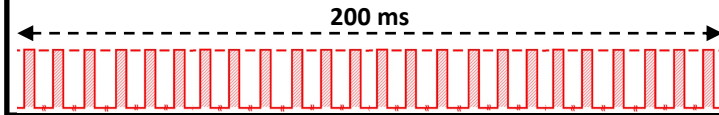
Dose = **10 Gy**

Dose Rate = **40 Gy/s**

Irradiation Time = **200 ms**

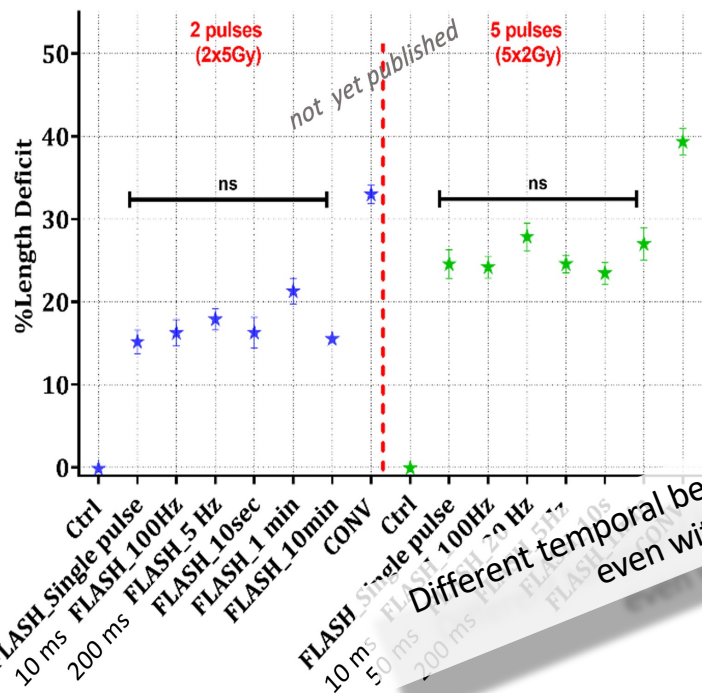
n. of pulses = **10^7 pulses**

$\bar{D}_0$ = **1 μ Gy**



Does only the average dose rate and total irradiation time matter?

% of Length deficit_Frequency variation_5.5MeV electrons_10Gy_4hpf



The overall time of irradiation does not matter But suggests that the dose delivered in the pulse does matter

Different temporal beam structures lead to different treatment outcomes even with the same Dose and Average Dose Rate

<https://www.biorxiv.org/content/10.1101/2024.04.19.590158v1.full>

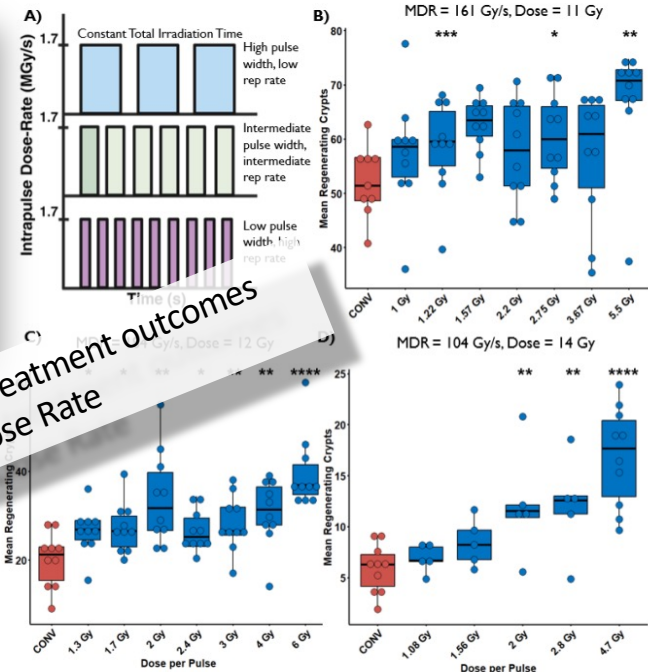


Fig. 2. (A) The beam structure schema (not to scale) illustrating how pulse width (PW) and pulse repetition frequency (PRF) are varied to achieve a delivery of different dose per pulse (DPP) while maintaining constant intrapulse dose rate, total irradiation time, mean dose rate (MDR), and total dose for each set of experiments in B-D. The mean number of regenerating crypts per circumference for mice receiving a total abdominal irradiation by either CONV - (0.3Gy/s, 10mGy/pulse, Red) or FLASH (Blue) to a dose of B) 11 Gy, MDR = 161 Gy/s, C) 12 Gy, MDR = 184 Gy/s, and D) 14 Gy, MDR = 104 Gy/s. An unpaired parametric t-test was used to compare the FLASH treated groups with the CONV treated group. * $p < 0.05$; ** $p < 0.01$; *** $p < 0.001$; **** $p < 0.0001$. For doses of 11-14 Gy and MDR of 104-184 Gy/s, sparing of crypts increases progressively with increasing DPP, especially at 14 Gy/104 Gy/s. At the lower doses/higher MDRs of 11-12Gy/161-184 Gy/s tested here; significant sparing of crypts is observed at DPPs > 1 Gy.

Courtesy of M.C. Vozenin (BelFLASH Symposium, Belgium, June 2024)

Realization of UHDR beams ...and related accelerators

Year	Radiation type	Machine	Energy (MeV)	Average dose rate (Gy/s)	Dose per pulse (Gy/pulse)	Pulse repetition rate (Hz)	Field size	Purpose	Dosimetry method
2020	Proton ³²	IBA isochronous cyclotron (USA)	227.5	130	N/A	106 MHz (quasi-continuous)	1.6 × 1.2 cm ² ellipse	Mouse (partial abdomen irradiation)	Plane-parallel IC, FC, MC simulation, EBT3 RCF
2020	Photon ³³	ANSTO Australian Synchrotron	0.07 and 0.09 mean	40–350 (at treatment depth and filtration)	200 (at 20 mm reference depth and filtration)	Continuous	2 × 2 cm (reference dosimetry size)	Rat study (brain cancer irradiation)	Pinpoint IC (reference), silicon semiconductor, and MC
2021	Proton ²⁵	Mevion synchrocyclotron (USA)	60	120–160	0.22 Gy/pulse (9.3 × 10 ³ Gy/s instantaneous)	750	Ø 1.1 cm FWHM (5 mm @ 90% isodose)	Feasibility of SOBP beam using a synchrocyclotron	IC, FC, MC simulation, and EBT-XD RCF
2021	Electron ³⁴	Varian Clinac 2100 C/D (USA)	10	240–260	0.81 Gy/pulse	360	Ø 1–1.5 cm	Feasibility of UHDR at the machine's isocenter	EBT-XD RCF
2021	Proton ³⁵	Research isochronous cyclotron (Germany)	68	75	N/A	20 MHz	Ø 1.3 cm	Preclinical setup for mouse irradiation	IC and RC
2021	Proton ³⁶	COMET ³⁸ isochronous cyclotron (Switzerland)	170–250	9000 (for a single spot)	N/A	72.85 MHz	~2.3–5 mm (16 × 1.2 cm ² by scanning)	Feasibility study	FC
2021	Helium ion ²⁶	Synchrotron (Germany)	145.74 MeV/u	185	N/A	Quasi-continuous	1 cm ² (by spot scanning)	In vitro study of dose, LET, and O ₂ concentration	Parallel-plate IC
2021	Carbon ion ²⁷	Synchrotron (Germany)	280 MeV/u	70	N/A	Quasi-continuous	1 cm ² (by spot scanning)	Dosimetry and in vitro study	IC and EBT3 RCF

e-

Research / modified clinical LINACs

p

Isochronous cyclotrons

p

Synchro cyclotrons

y
ions

Synchrotrons

F. Romano *et al.* Med. Phys. (2022)

Challenges of dosimetry for electron UHDR beams

First studies on **ion recombination** for commercially available chambers → **determining ion collection efficiency**

Petersson et al., Med Phys 44 (2017) 1157

High dose-per-pulse electron beam dosimetry — A model to correct for the ion recombination in the Advanced Markus ionization chamber

Kristoffer Petersson,^{a)} Maud Jaccard, Jean-François Germond, Thierry Buchillier, and François Bochud

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Jean Bourhis and Marie-Catherine Vozenin

CHUV, Service de Radio-Oncologie, Rue du Bugnon 46, CH - 1011 Lausanne, Switzerland

Claude Bailat

CHUV, Institut de Radiophysique, Rue du Grand-Pré 1, CH-1007 Lausanne, Switzerland

Kranzer et al., Medical Physics, 48 (2), February 2021

Ion collection efficiency of ionization chambers in ultra-high dose-per-pulse electron beams

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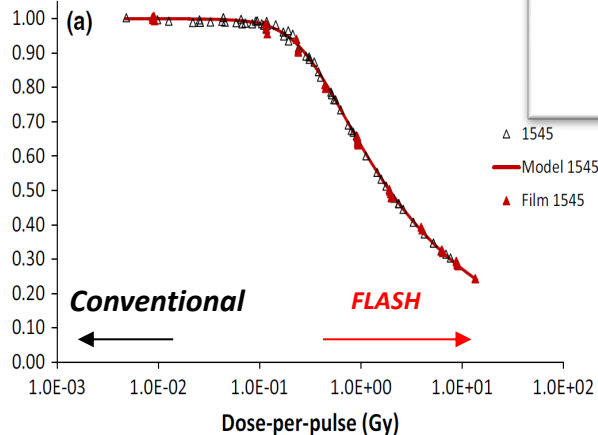
(Received 19 June 2020; revised 30 September 2020; accepted for publication 18 November 2020; published 2 January 2021)



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$k_s = 1/(\text{ion coll. eff.})$



A. Bourgouin Phys. Med. Biol. 68 (2023) 235002

PAPER

Charge collection efficiency of commercially available parallel-plate ionisation chambers in ultra-high dose-per-pulse electron beams

Alexandra Bourgouin^{1,*}, Jose Paz-Martín², Yunus Can Gedik³, Franziska Frei⁴, Peter Peier⁴, Séverine Rosomme⁵, Andreas A Schönfeld⁶, Andreas Schüller¹, Faustino Gomez Rodriguez² and Ralf Peter Kanch¹

UHDR proton beams (isochronous cyclotrons)

IBA, Varian, Hitachi

Isochronous cyclotron (quasi-continuous radiation)
($f=72.8$ MHz, 2nd Harmonic)

$$\dot{d} < 2 \text{ kGy/s}$$



Average DR 100-400 Gy/s

Received: 2 March 2022 | Revised: 20 June 2022 | Accepted: 27 June 2022

DOI: 10.1002/mp.15844

RESEARCH ARTICLE

MEDICAL PHYSICS

Ultrahigh dose rate pencil beam scanning proton dosimetry using ion chambers and a calorimeter in support of first in-human FLASH clinical trial

Eunsin Lee^{1,2} | Ana Mónica Lourenço^{3,4} | Joseph Speth⁵ | Nigel Lee³ | Anna Subiel³ | Francesco Romano⁶ | Russell Thomas^{3,7} | Richard A. Amos⁴ | Yanbiao Zhao^{1,2} | Zhijian Viao^{1,2} | Anthony Meesaie^{1,2}



Contents lists available at ScienceDirect

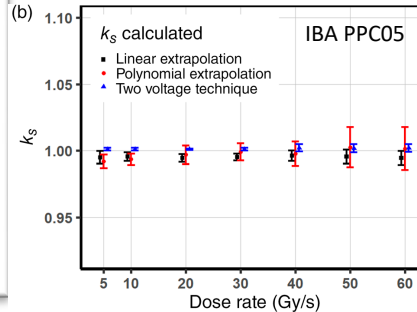
Physica Medica

journal homepage: www.elsevier.com/locate/ejmp

Ion recombination correction factors and detector comparison in a very-high dose rate proton scanning beam

A.M.M. Leite^{a,b,*}, M. Cavallone^b, M.G. Ronga^b, F. Tromprier^c, Y. Ristic^c, A. Patriarca^b, L. De Marzi^{b,d,*}

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Average dose rate 5-60 Gy/s

Chambers:

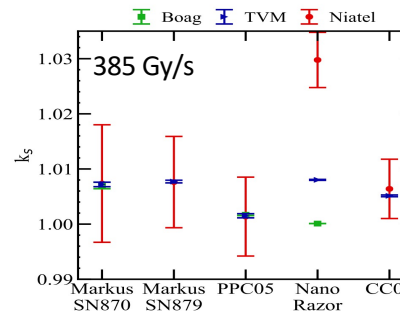
PTW Advanced Markus
IBA PPC05

PPC05

K_{sat} : **1.002**

Adv Markus

K_{sat} : **1.001-1.006**



Average dose rate 4 Gy/s - 385 Gy/s

Instantaneous dose rates:

up to 1000 Gy/s

Chambers:

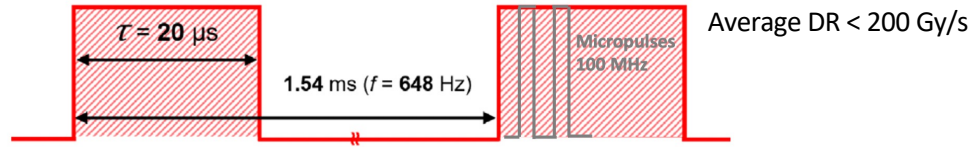
Razor Nano-chamber CC01,
PTW Advanced Markus, PPC05

UHDR proton beams (synchrocyclotrons)

IBA, Mevion

Synchrocyclotron (FLASH dose rate)

$$\dot{d} < 10 \text{ kGy/s}$$



Feasibility of proton FLASH irradiation using a synchrocyclotron for preclinical studies

Arash Darafsheh¹⁾ and Yao Hao

Department of Radiation Oncology, Washington University School of Medicine, St. Louis, MO 63110, USA

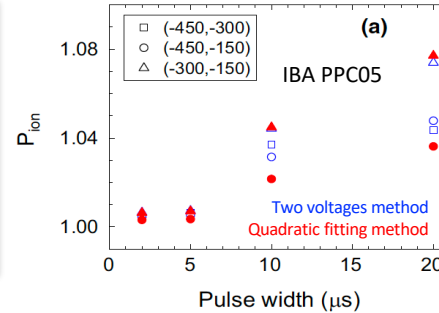
Townsend Zwart, Miles Wagner, and Daniel Catanzano

Mevion Medical Systems, 300 Foster St., Littleton, MA 01460, USA

Jeffrey F. Williamson, Nels Knutson, Baozhou Sun, Sasa Mutic, and Tianyu Zhao

Department of Radiation Oncology, Washington University School of Medicine, St. Louis, MO 63110, USA

(Received 7 January 2020; revised 15 May 2020; accepted for publication 15 May 2020; published 15 June 2020)



230 MeV **passive** proton beam

Average dose rate: **100-200 Gy/s**,

Instantaneous: dose rate **$1.66 \cdot 10^4 \text{ Gy/s}$**

Pulse duration: **2-20 μs**

Received: 3 January 2021 | Revised: 25 May 2021 | Accepted: 26 May 2021

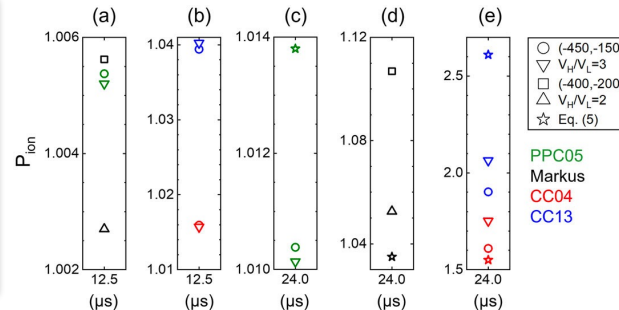
DOI: 10.1002/mp.15021

RESEARCH ARTICLE

MEDICAL PHYSICS

Spread-out Bragg peak proton FLASH irradiation using a clinical synchrocyclotron: Proof of concept and ion chamber characterization

Arash Darafsheh¹ | Yao Hao¹ | Xiandong Zhao¹ | Townsend Zwart² | Miles Wagner² | Tucker Evans² | Francisco Reynoso¹ | Tianyu Zhao¹



Chambers: PPC05, Markus

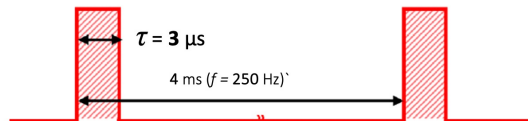
K_{sat} : **1.003–1.1**

UHDR electron beams (LINAC)

Average DR < 200-700 Gy/s

Clinical LINAC for Radiotherapy (modified)

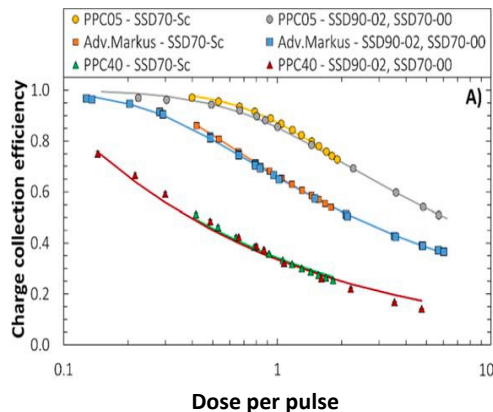
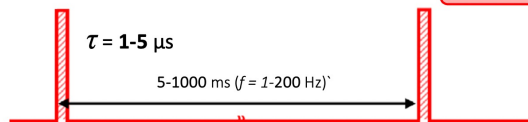
$\dot{d} < 100$ kGy/s



Average DR < 2 kGy/s

Research LINAC for pre-clinical studies

$\dot{d} < 5$ MGy/s



Modified clinical LINACS

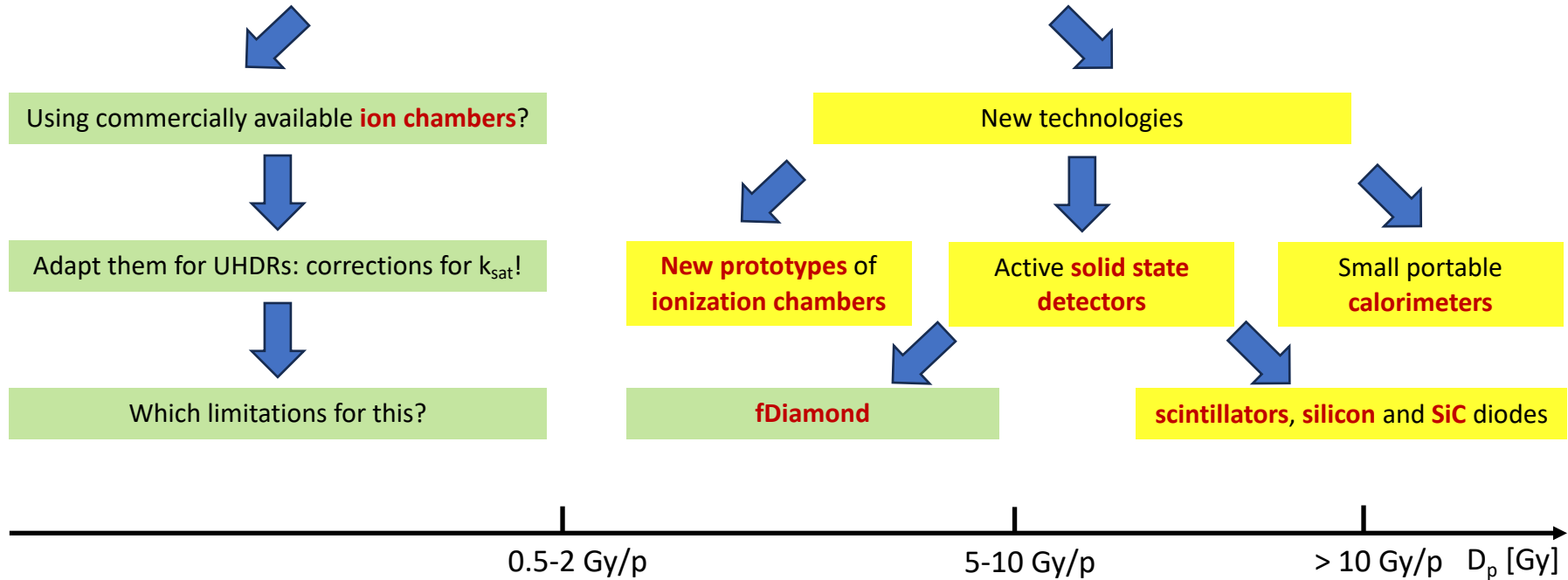
Research LINACS

TABLE I. Characteristics of currently available electron devices.

	Kinetron (CGR-MeV/ PMB-Alcen)	Oriatron eRT6 (PMB-Alcen)	Oxford linac	Modified Varian (Stanford)	Modified Elekta	Mobetron (IntraOp)	FLASH-knife (PMB-Alcen)	SIT (Sordina)	FLEX (RadiaBeam)	PITZ
Available beam energy (MeV)	4.5	5	6	17	8 and 10	6 and 9	6–10	5–12	9	22
Maximum average dose rate (Gy/s)	2500	1000	1500	750	≥300	>700 at 6 MeV, >800 at 9 MeV	Up to 350 Gy/s at 30 mm depth	1500	7500	10 000
Maximum dose per pulse (Gy)	6.3	12	5	3	1.9	>8 at 6 MeV, >9 at 9 MeV	...	18.2	>25	1000
Max. beam size for at least 1.5 Gy/pulse (cm)	5	20.5 (FWHM)	5 (FWHM)	5	2 (5% flatness)	6 at 90%	...	1.3 (FWHM)	6	15
Max. beam size at max. dose rate (cm)	0.012	0.5	...	5	2 (5% flatness)	4 at 90%	...	0.5 (FWHM)	6 (FWHM)	2
Short-term stability (%)	...	<1	...	<2	1 to 4	0.8	...	...	±2%	<1%
Long-term stability	...	4.1%	...	~4%	...	1.8 at 6 MeV, 2.3 at 9 MeV	...	...	±2%	<1%
Commissioning reference(s)	Lansonneur <i>et al.</i> (2019)	Petersson <i>et al.</i> (2017), Jaccard <i>et al.</i> (2018), and Jorge <i>et al.</i> (2019)	...	Schueler, Trovati <i>et al.</i> (2017)	Lempart <i>et al.</i> (2019)	Moeckli <i>et al.</i> (2021)	...	Di Martino <i>et al.</i> (2020)	Kutsaev <i>et al.</i> (2021)	Stephan <i>et al.</i> (2022)
FLASH effect validated	Favaudon <i>et al.</i> (2014), Vozenin <i>et al.</i> (2019), and Fouillade <i>et al.</i> (2020)	Montay-Gruel <i>et al.</i> (2017, 2019, 2020, 2021), Vozenin <i>et al.</i> (2019), Alaghband <i>et al.</i> (2020), Allen <i>et al.</i> (2020), Limoli <i>et al.</i> (2020), Chabi <i>et al.</i> (2021), Kacem <i>et al.</i> (2022), and Rohrer Bley <i>et al.</i> (2022)	Ruan <i>et al.</i> (2021)	Simmons <i>et al.</i> (2019), Levy <i>et al.</i> (2020), Y.-E. Kim <i>et al.</i> (2021), and Eggold <i>et al.</i> (2022)	No	Valdes Zayas <i>et al.</i> (2023)	No	No	No	No
Dosimetrically intercompared	Dismantled in 2020	Gonçalves Jorge <i>et al.</i> (2022)	No	Gonçalves Jorge <i>et al.</i> (2022)	No	No	No	No	No	No
Biologically intercompared	Dismantled in 2020	Yes	No	Yes	No	No	No	No	No	No

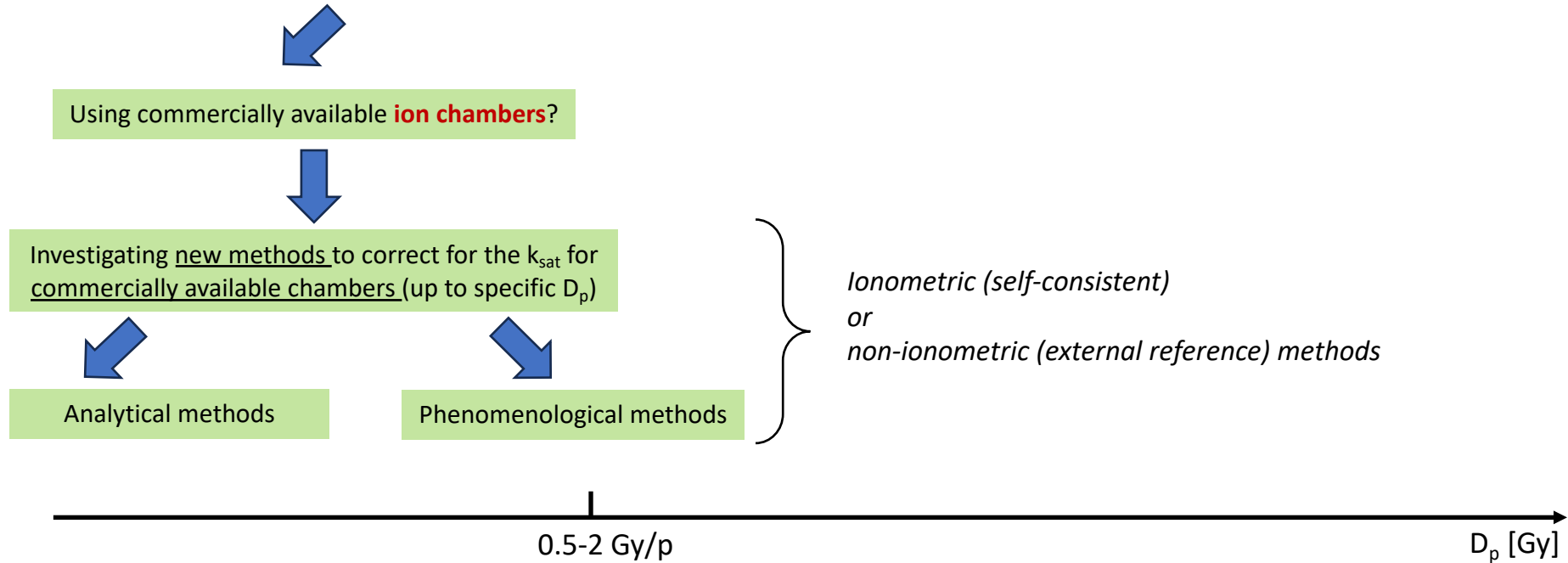


What's the current status of instrumentation for UHDRs?

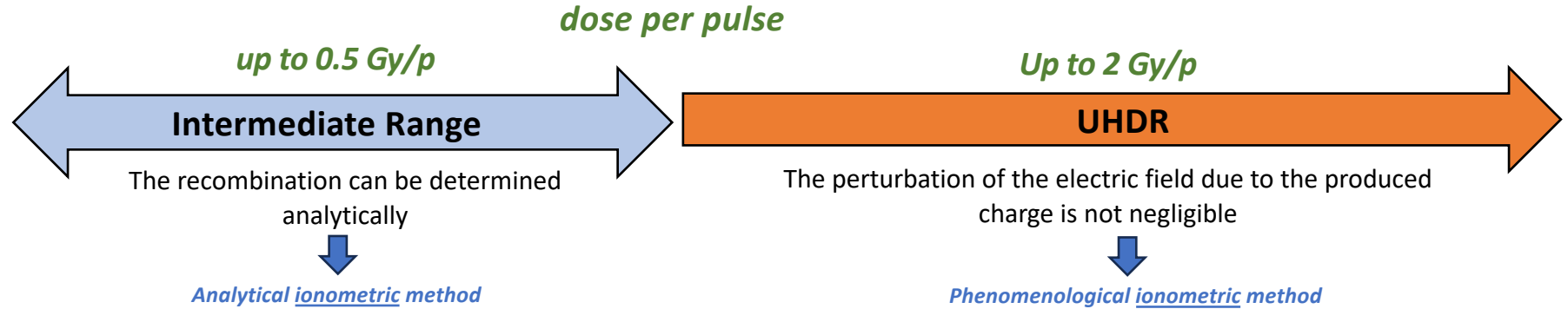




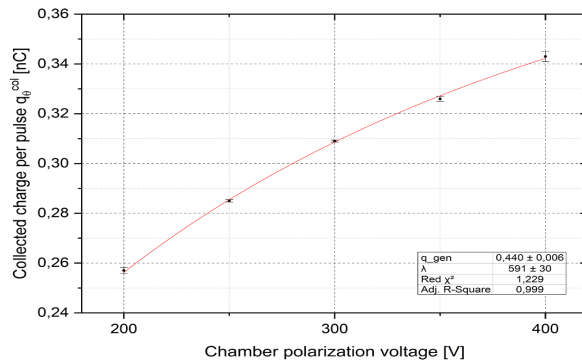
What's the current status of instrumentation for UHDRs?



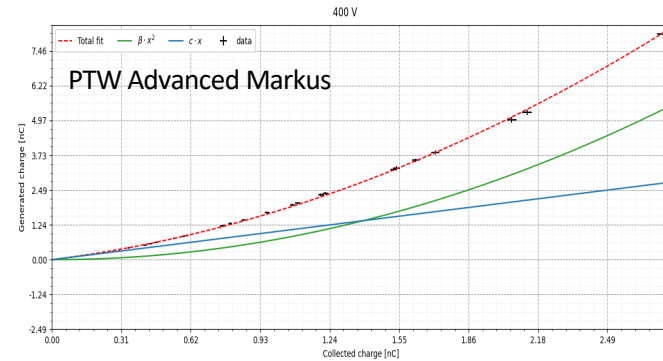
Ionization chambers: determine the ion rec corr (ksat) for commercial chambers



F. Di Martino et al., Physica Medica 103 (2022) 175–180

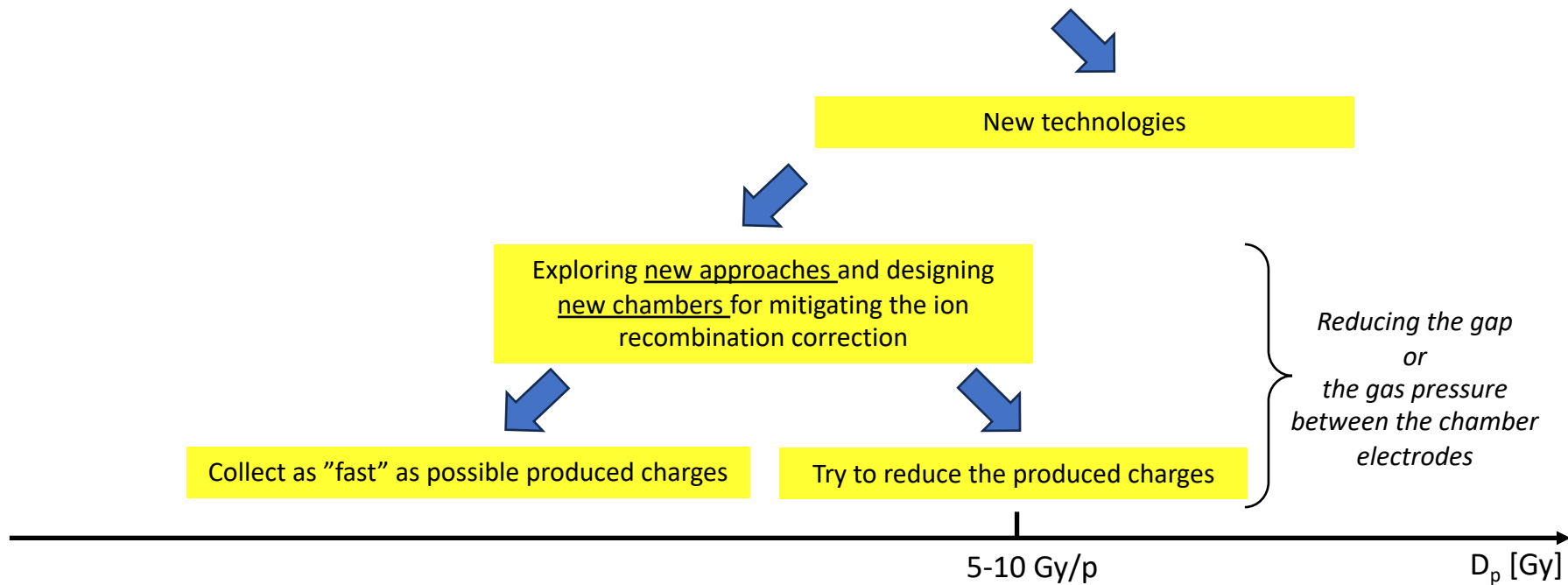


L. Masturzo et al., Med. Phys., under review





What's the current status of instrumentation for UHDRs?



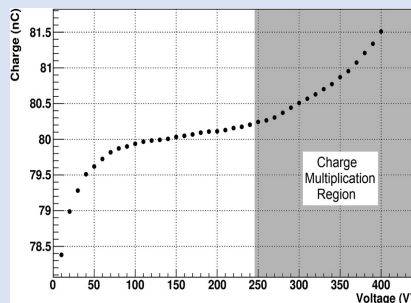
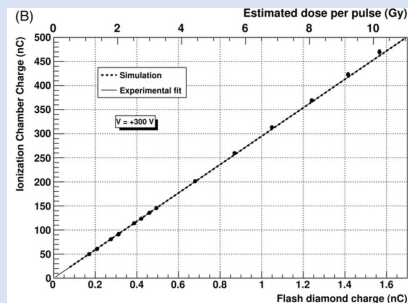
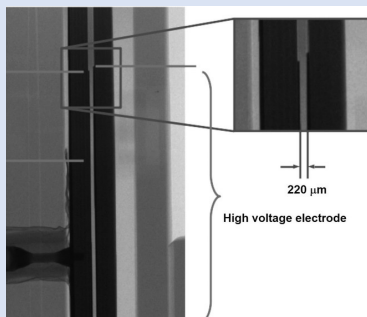
Challenges of dosimetry for electron UHDR beams

New approaches and chamber designs for decreasing ion recombination on new prototypes

Ultra-thin ionization chambers

F. Gomez et al., Med. Phys. 2022

R Kranzer et al., Physica Medica 104 (2022) 10–17



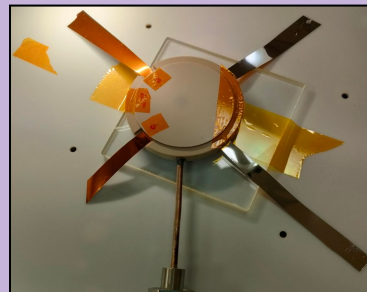
USC (University of Santiago De Compostela)

Noble gas filled ion chamber: the ALL chamber

F. Di Martino et al., EJMP 2022

Fill the cavity with a **noble gas** to prevent the **capture of electrons** and then the production of negative ions which are responsible of the ion recombination (and decreasing gas pressure)

1st prototype

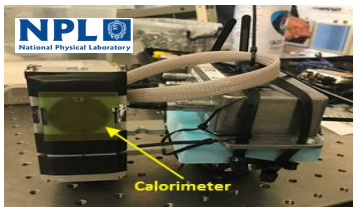


2nd prototype

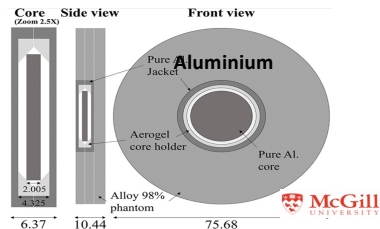


- ✓ 2nd prototype filled with N₂ gas at 1 bar, 500 mbar, 100 mbar
- ✓ First tests with 9 MeV UHDR at CPFR show linearity up to **5 Gy/pulse** at 100 mbar pressure

INFN Pisa Division, CPFR and USC



F. Romano et al., Journ. of Phys. (2020)
S. Mc Callum et al., App. Science (2023)



Bourgouin et al., Front. In Phys., 2020

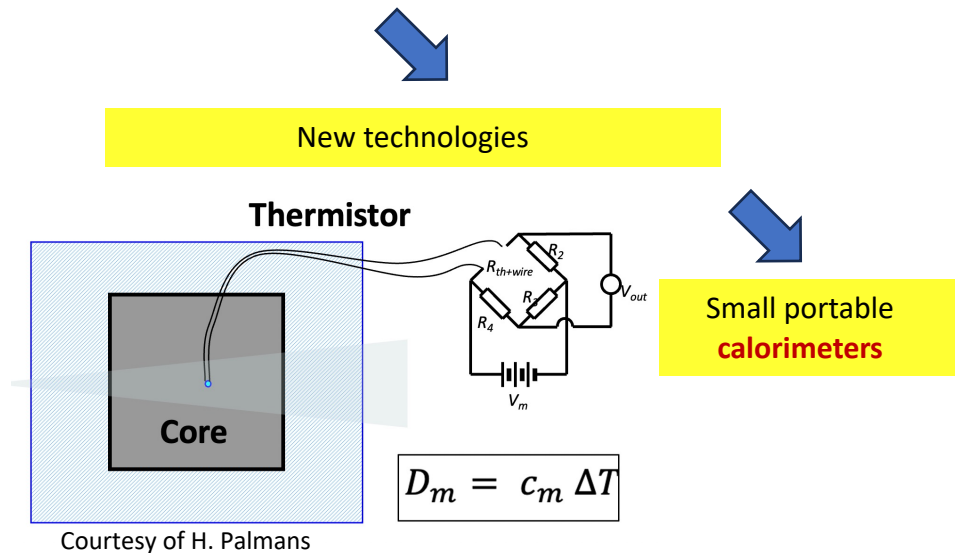
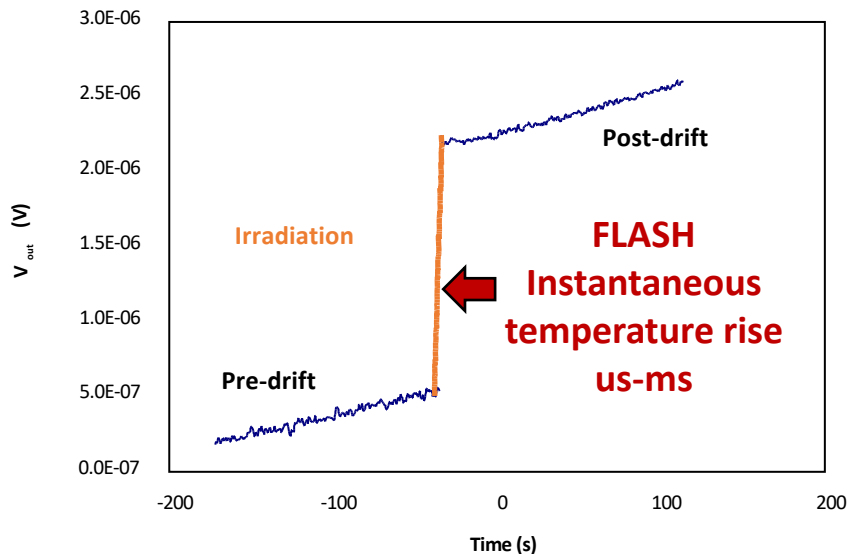


Bourgouin et al., Med Phys. 2022;49:6635–6645



G. Bass et al., Br. J. Radiol. (2023)

What's the current status of instrumentation for UHDRs?



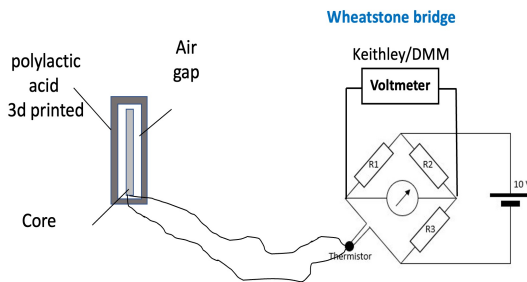
> 10 Gy/p D_p [Gy]

Test of the calorimeter with UHDR electron beams @ CPFR in Pisa

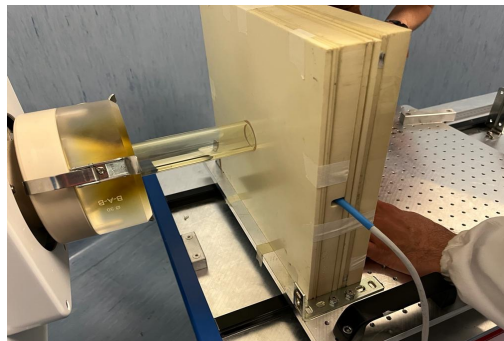
G. Bass et al., Br. J. Radiol. (2023)



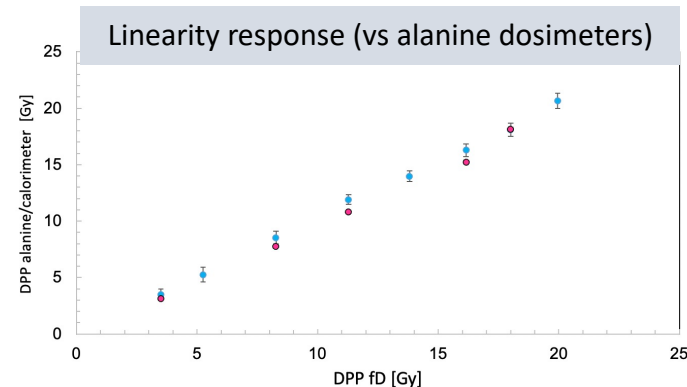
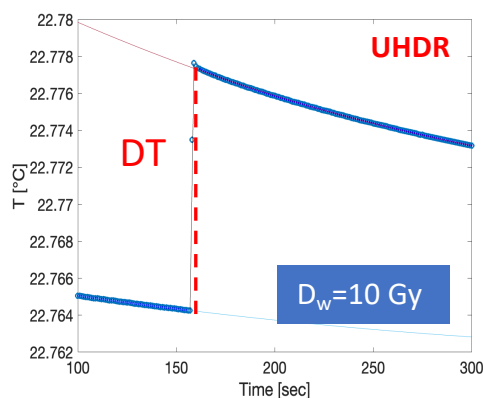
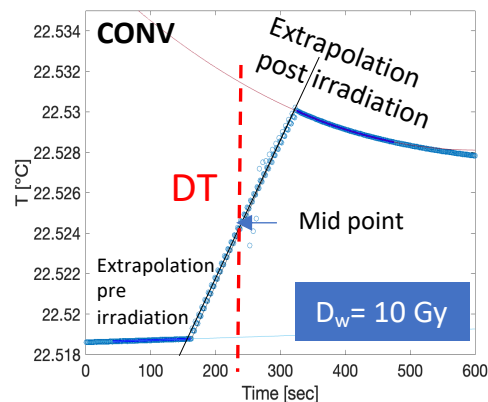
- Developed by NPL
- Simple usage and low cost
- 2 mm graphite core
- 1 single thermistor connected to the Wheatstone bridge
- IBA PPC05 ion chamber geometry (same holders)



- Tested at CPFR with the SIT ElectronFLASH LINAC
- $E = 9 \text{ MeV}$; **single pulse duration: 4 μs**



- **Dose per pulse: from 0.1-6 Gy**
- **IDR up to 2 MGy/s**
- **Repetition frequency: 1-245 Hz**

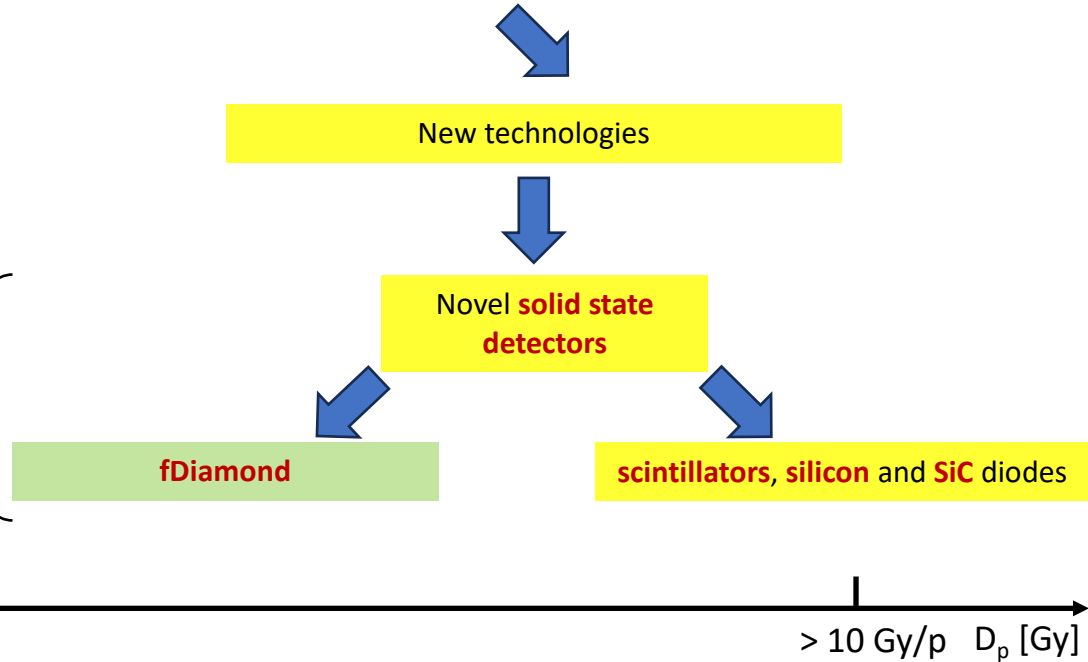


Tested also with UHDR proton beams

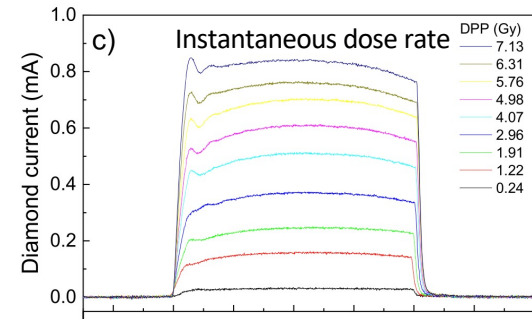
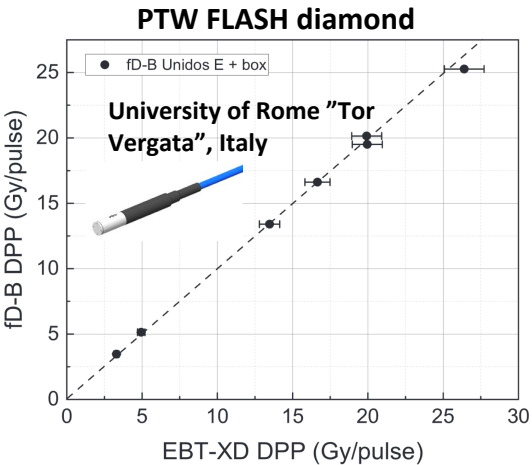


What's the current status of instrumentation for UHDRs?

- *Reference and small field dosimetry*
- *Relative dosimetry*
- *Pulse structure measurements (IDR)*



fDiamond for reference dosimetry and IDR measurements

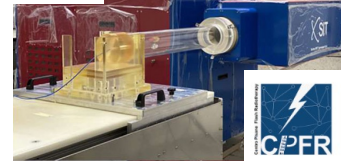


- Linear response at UHDRs
- pulse structure measurements
- High spatial resolution ($\ll 1$ mm)

Table 1. The summary of devices and their applications in UHDR beams.

Device/instrument	UHDR beam modality	Energy (MeV)	DPP (Gy)	Instantaneous dose rate ($\text{Gy } \mu\text{s}^{-1}$)	Average dose rate (Gy s^{-1})	Pulse duration (μs)	Pulse repetition rate (Hz)	Standard uncertainty	Availability	References
Potential secondary/tertiary standards										
UTIC	Electrons	9 20	1–10 1.2–5.4	0.25–2.5 0.48–2.2	10–100 6–27	4 2.5	10 5	1.40%	Under development	(Kranzer <i>et al</i> 2021) (Gómez <i>et al</i> 2022) figure 3
Alanine	Electrons	20	0.15–9	0.15–3.3	0.75–45	1.35, 2.5, 2.7	5	0.85%	Commercial (through calibration laboratories)	(Bourgouin <i>et al</i> 2023a) Figure 4
flashDiamond	Electrons	7, 9 20	0.3–26 0.2–10	0.5–6.6 0.15–3.3	Up to 960 1–50	1–4 1.35–3	5–245 5	1% @ 0.25 $\text{Gy } \mu\text{s}^{-1}$ 3% @ 2.5 $\text{Gy } \mu\text{s}^{-1}$	Commercial	(Kranzer <i>et al</i> 2022a) (Marinelli <i>et al</i> 2022) (Marinelli <i>et al</i> 2023) (Tessonnier <i>et al</i> 2023) (Verona Rinati <i>et al</i> 2022) (Di Martino <i>et al</i> 2023) figure 5
SiC diode	Electrons	20 9	0.4–11 0.02–5	0.7–3.8 0.01–1.2	2–55 0.6–53	2.9, 1.6, 0.5 2, 4	5 30	3% —	Under development	(Fleta 2024) (Romano <i>et al</i> 2023) (Milluzzo <i>et al</i> 2023)
Aerrow graphite probe calorimeter	Electrons	20	0.6–5.6	0.24–2.24	3–28	2.5	5	1.06%	Commercial	(Bourgouin <i>et al</i> 2023b)
Commercially available ionization chambers	Electrons Protons (PBS)	20 227	0.14–6.2 4.3, 17.5, and 38.1	0.352–2.48 4×10^4 – 6×10^4 3.85×10^4 –3	0.7–31 4–385	2.5 1×10^4 – 6×10^4 99×10^3	5 Single pulse (PBS)	2.5% up to 10% ^a 1.5% ^b	Commercial	(Bourgouin <i>et al</i> 2023b) (Leite <i>et al</i> 2023)

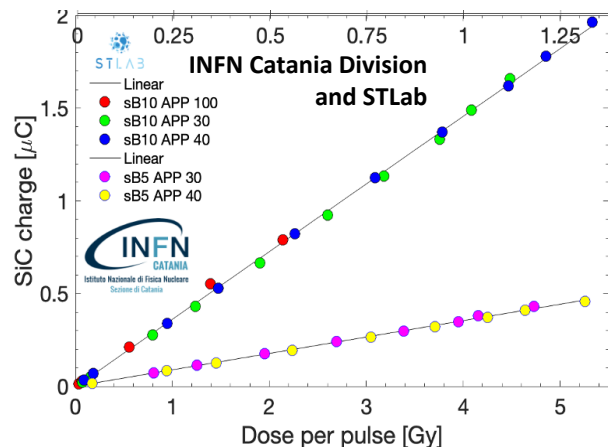
Response of other active solid-state detectors a UHDRs



- Linear response at UHDR
- High spatial resolution ($< 1 \text{ mm}$) $\rightarrow$ small fields
- Good stability (long-term response stability?)
- Water equivalence
- Possibility for 2D configurations
- Encapsulation to be used in reference conditions



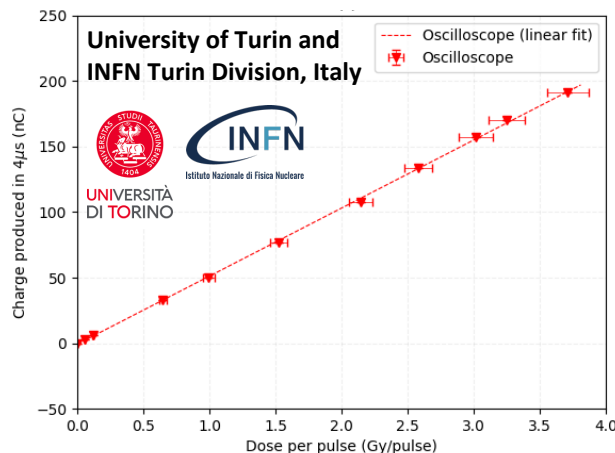
SiC detectors



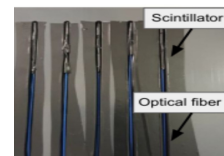
F. Romano et al. Appl. Phys. (2023)
G. Milluzzo et al. (2024)
C. Okpuwe et al 2025 Rad. Res. (2025)



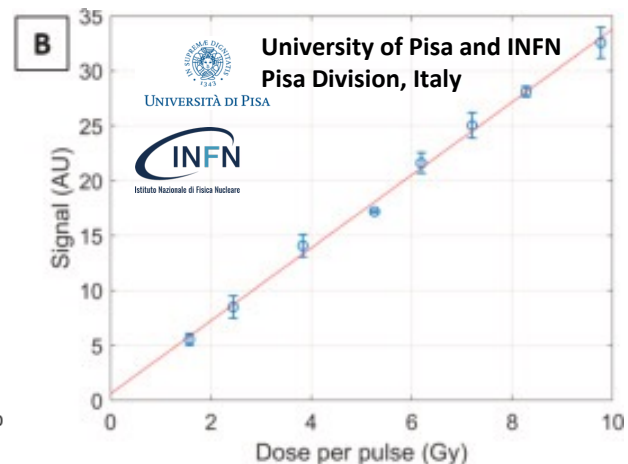
Silicon detectors



E. Medina et al., Frontiers in Physics (2022)



Scintillators/scintillator fibers

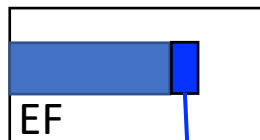


M. Morrocchi et al. JINST (2022)
E. Ciarrocchi et al., Physica Medica (2024)

Beam pulse structure / IDR measurements:

bergoz
INSTRUMENTATION

ACCT (AC current transformer)



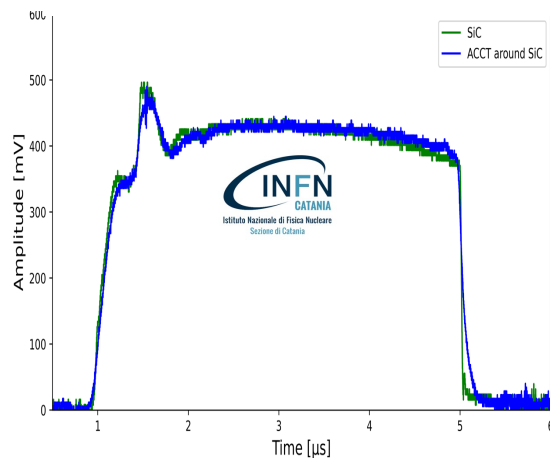
App 40

SiC/Silicon/Scintillators



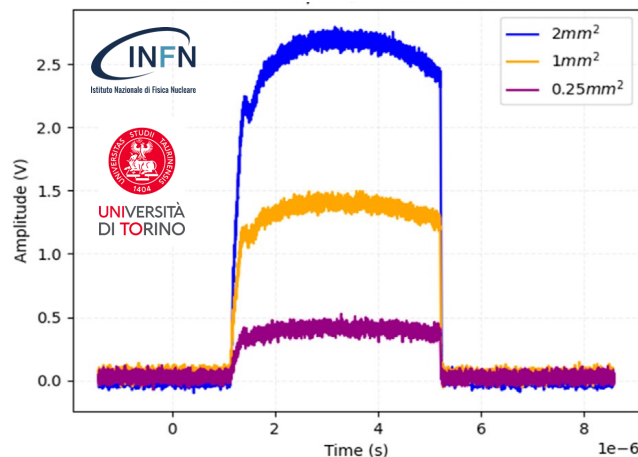
ACCT

SiC detectors



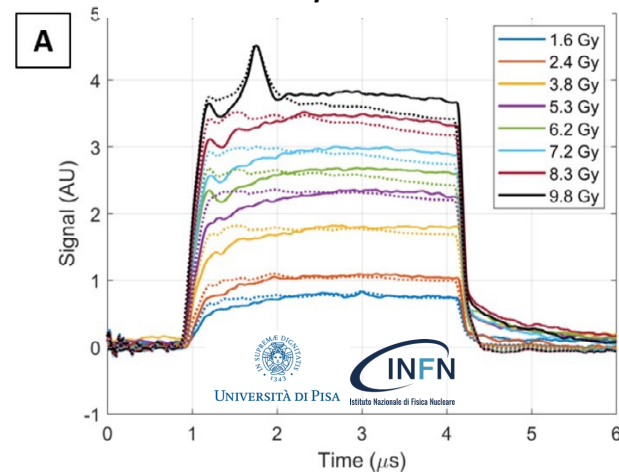
F. Romano et al. Appl. Phys. (2023)
G. Milluzzo et al. (2024)
C. Okpuwe et al 2025 Rad. Res. (2025)

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E. Medina et al., Frontiers in Physics (2022)

Scintillators/scintillator fibers



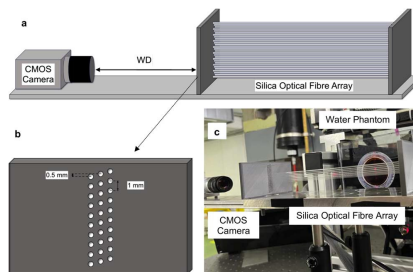
M. Morrocchi et al. JINST (2022)
E. Ciarrocchi et al., Physica Medica (2024)

QA devices to support clinical trials (and address radiation protection issues?)

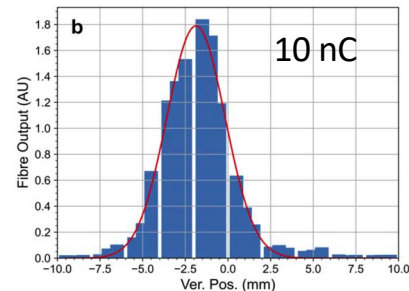
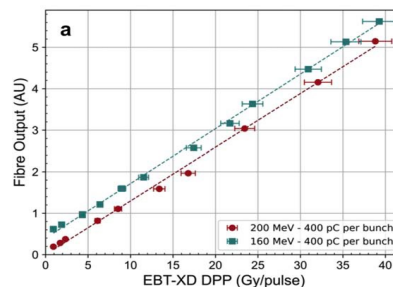
Multi scintillating fibers

- 28 fused silica optical fibres
- 0.4mm in diameter
- 30 cm length

clear



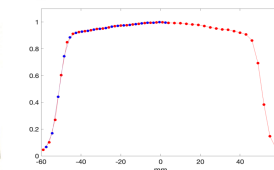
Joseph J Bateman et al 2024 Phys. Med. Biol. 69 085006



SiC 1D geometrical configurations for real time dose profile measurements (**DREAM**)



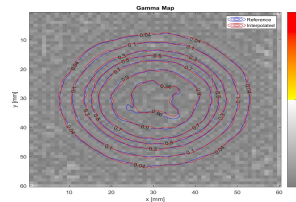
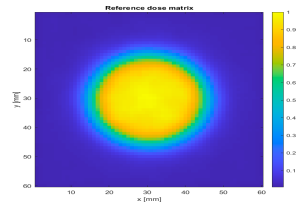
R4 Research for Innovation



Università degli Studi di Palermo



SiC 2D geometrical configurations for real time dose map measurements (**DALI'**)



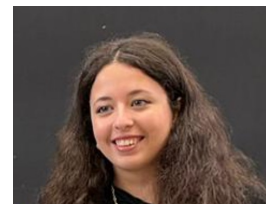
Final considerations

- Huge effort in the last years on **characterizing technologies for dosimetry** and develop **new approaches**
- The final goal is probably less challenging than it was thought at the beginning (20-30 Gy/p vs few Gy/p)
- Now clinical trials push physicists to address new challenges:
 - **Compare performances** of dosimeters with dedicated experiments at the same conditions
 - **Small field** dosimetry, **pulse structure** characterization, **radiation protection** ...most suitable technology
 - Understanding which developed dosimeters are “useful” for **medical physicist** and for which cases
- Dosimetry:
 - Less critical for **proton beams**: small corrections for isochronous cyclotrons, larger with synchrocyclotrons
 - More effort required for **electron beams** (Linacs):
 - **commercial ion chambers** reliably used with correction methods up to 2 Gy/p: to be also used for Linac output periodic checks (**new chamber prototypes** under development for higher Dpp)
 - **calorimeters** for higher Dpp or stability check for novel detectors (semiconductors) and commissioning
 - **Solid state detectors** for relative dosimetry, small field dosimetry, temporal reconstruction (IDR)
 - **2D systems** (**scintillators**, **semiconductors**,...) for: i) QA; ii) addressing radiation protection issues; iii) (in a future perspective) dosimetric check of treatment plans
- Protocols and current initiatives : **AAPM** task group 359, **ESTRO** FLASH FOCUS Group, **AIFM** (for low E e-)



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