

National Research Nuclear University «Moscow Engineering Physics Institute»

**Optimization of the gamma - locator characteristics  
based on the SiPM**

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## Radiopharmacological $\gamma$ - diagnostics

- One of the main problems - localization of the  $\gamma$ -rays sources in a biological object.
- $\gamma$ -diagnostics used in the search of local tumor formations (seal). RFP ( $\gamma$ -source) is introduced into the body and concentrates in malignant tumors.  $\gamma$ -ray detector allows us to localize the place formation.
- One such possible devices can be designed as a detector for  $\gamma$ -rays.
- For these tasks a  $\gamma$ -ray detector in the energy range 60 ~ 600 keV is required.

## Abstract.

The results of studies on the optimal scintillator - photodetector (SiPM) pair for gamma - locator device are presented.

The criterion is the maximum ratio of the signal / background for gamma - rays with energies in the range  $60 \div 660$  keV. The optimal pair consists of a scintillator LaBr<sub>3</sub>: Ce and SiPM firm HAMAMATSU.

The experimentally obtained signal / background ratio  $\sim 1000$ .

<sup>137</sup>Cs & <sup>241</sup>Am sources activity is  $\sim 10^5$  Bk.

Gamma - Locator - a medical device based on the SiPM for operative cancer diagnostics

SiPM - Silicon photomultipliers

**We were investigating and made:**

- choice of the optimal pair of scintillator + photodetector
- electronics assembly for the gamma - rays detection in the energy range from 60 to 660 keV
- processing of the physical experiments data
- testing and debugging of the detector prototype

## Experimental setup

Fig.1. shows a diagram of the experimental setup the measurements were taken on.

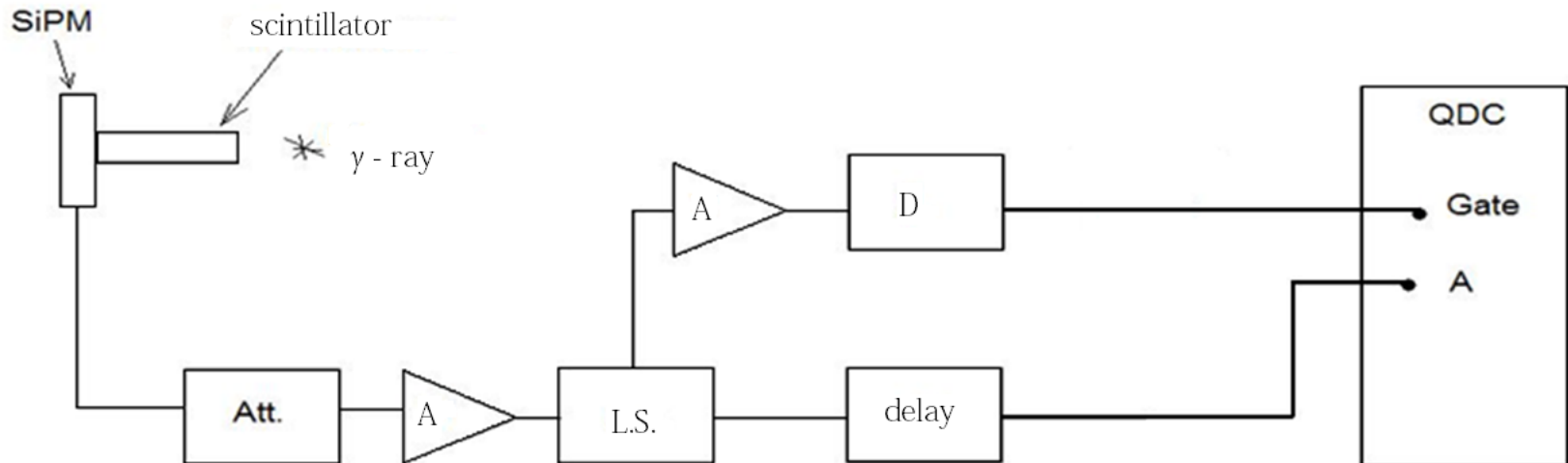
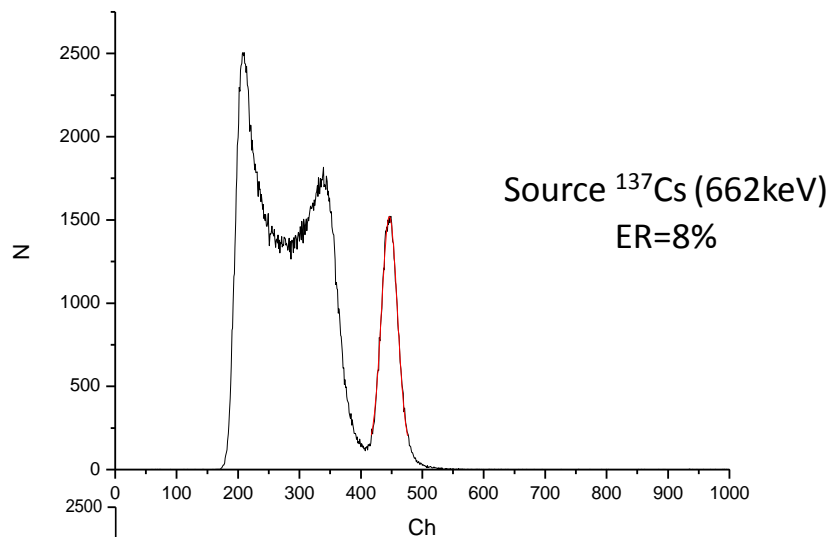


Fig.1. SiPM- photodetector; scintillator– LYSO, LaBr3Ce; Att.- attenuator; A.- amplifier; L.S.- linear splitter; D.- discriminator; QDC (Lecroy2249).

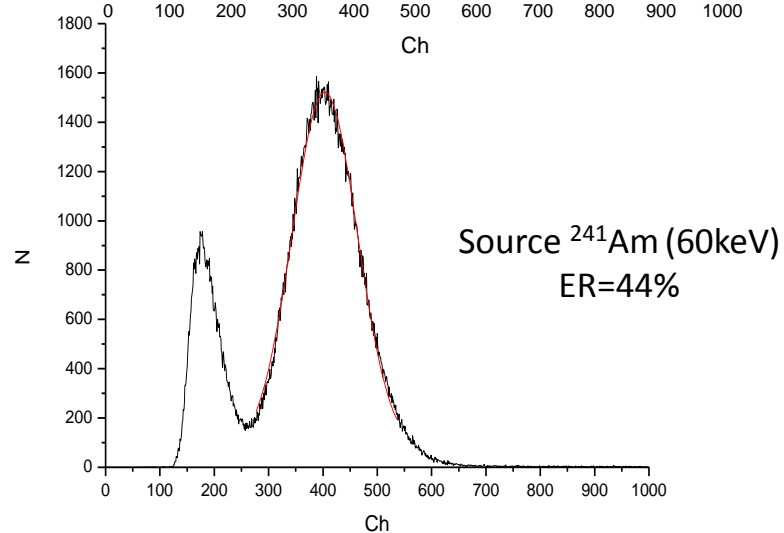
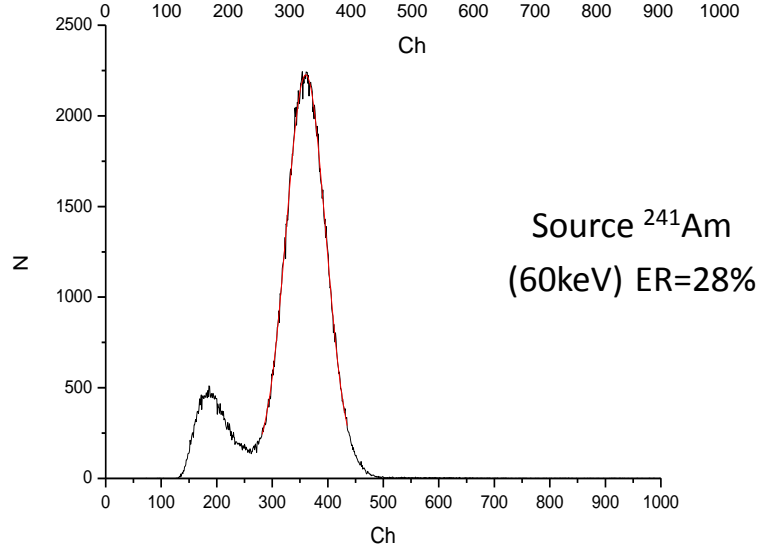
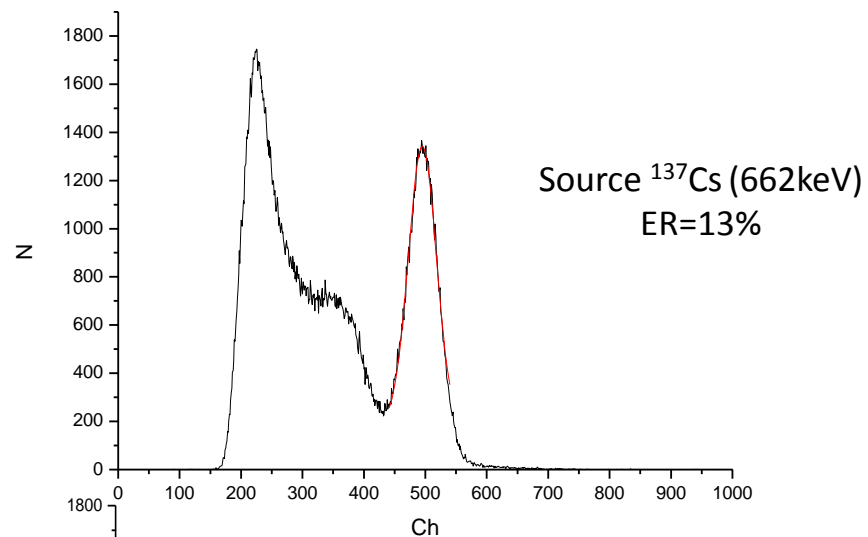
# Achieved experimental results

## SiPM MPPC Hamamatsu 3x3 spectra;

LaBr<sub>3</sub>:Ce scintillator;

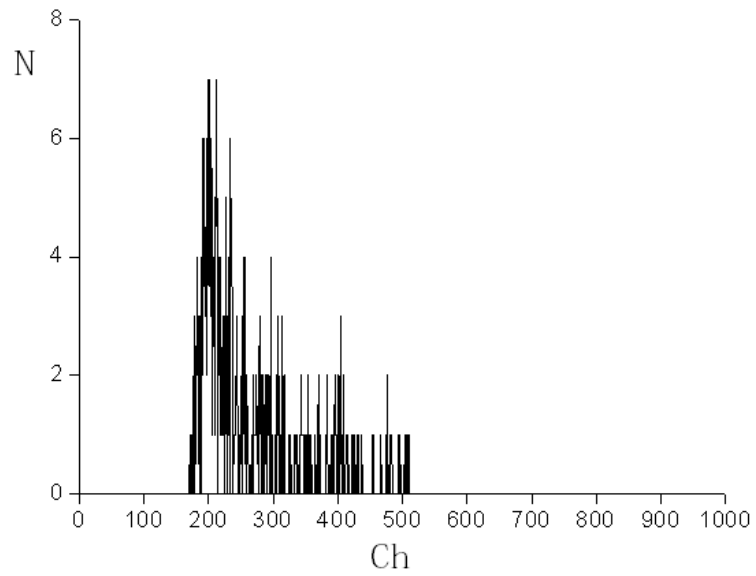


LYSO scintillator;

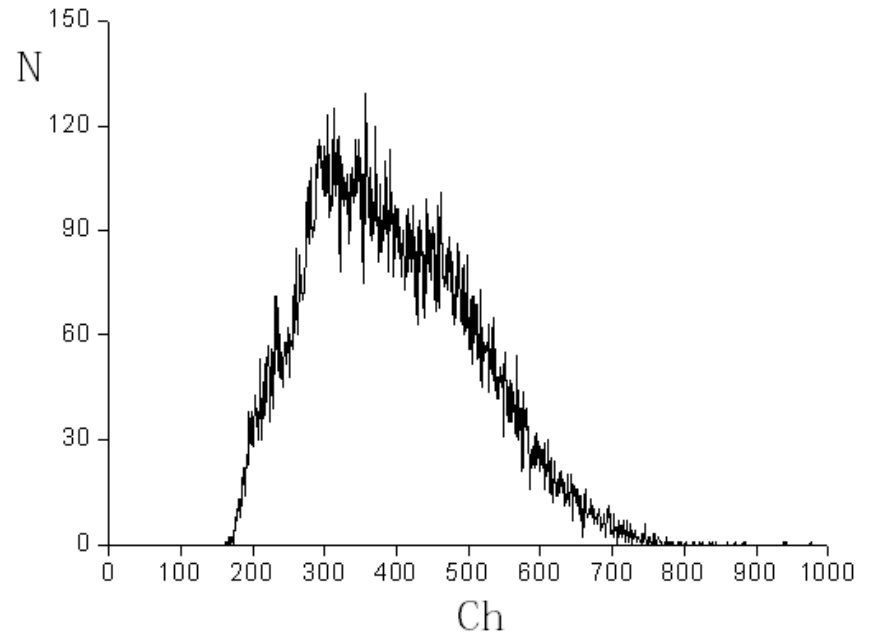


**Fig.2. Experimental spectra.**

## Background for $\text{LaBr}_3:\text{Ce}$ and LYSO scintillators.



**Background for  $\text{LaBr}_3:\text{Ce}$  scintillator**



**Background for LYSO scintillator**

Table 2. Experimental measurement results

| Photodetector              | crystal LaBr <sub>3</sub> :Ce |                  |                   |                  |
|----------------------------|-------------------------------|------------------|-------------------|------------------|
|                            | <sup>137</sup> Cs             |                  | <sup>241</sup> Am |                  |
|                            | ER,%                          | N1/N2(photopeak) | ER,%              | N1/N2(photopeak) |
| <i>SiPM MPPC Hamamatsu</i> | <b>8</b>                      | <b>3700</b>      | <b>28</b>         | <b>770</b>       |
| SiPM MAPD-3 (Zecotek)      | 16                            | 1070             | 45                | 414              |
| SiPM MEPhI                 | 13                            | 2803             | 44                | 2718             |
| Photodetector              | crystal LYSO                  |                  |                   |                  |
|                            | <sup>137</sup> Cs             |                  | <sup>241</sup> Am |                  |
|                            | ER,%                          | N1/N2(photopeak) | ER,<br>%          | N1/N2(photopeak) |
| <i>SiPM MPPC Hamamatsu</i> | <b>13</b>                     | <b>13</b>        | <b>44</b>         | <b>977</b>       |
| SiPM MAPD-3 (Zecotek)      | 16                            | 16               | 52                | 605              |
| SiPM MEPhI                 | 17                            | 11               | 56                | 1023             |



## GAMMA-LOCATOR PRACTICAL IMPLEMENTATION

A prototype of a compact device was designed and manufactured to work with the real short half life sources (Fig. 3); the detector itself (Fig. 4)

The measurement results shown on Fig. 5.6 allow us to estimate the accuracy of the  $\gamma$  - quanta source coordinates measurement.

Measurements duration is 5 seconds. Collimator with 2 mm diameter was used.



Fig.3. Detector



Fig.4. Gamma-locator prototype

Fig.5. The counting rate dependence of the source ( $^{137}\text{Cs}$ ) - detector distance; **a** – air, **b** – using absorber(water), **c** - noise

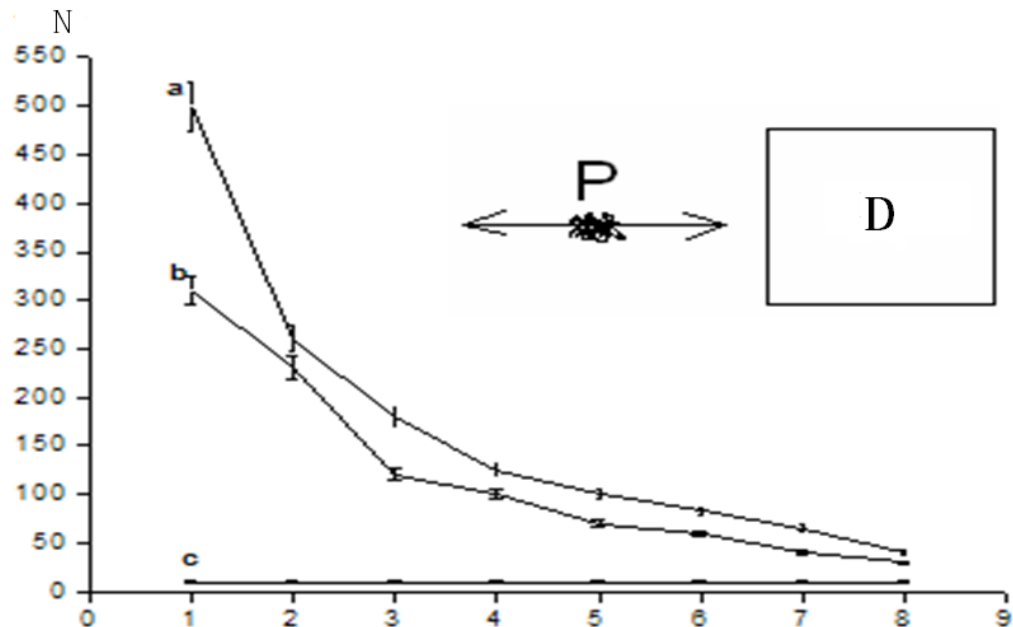
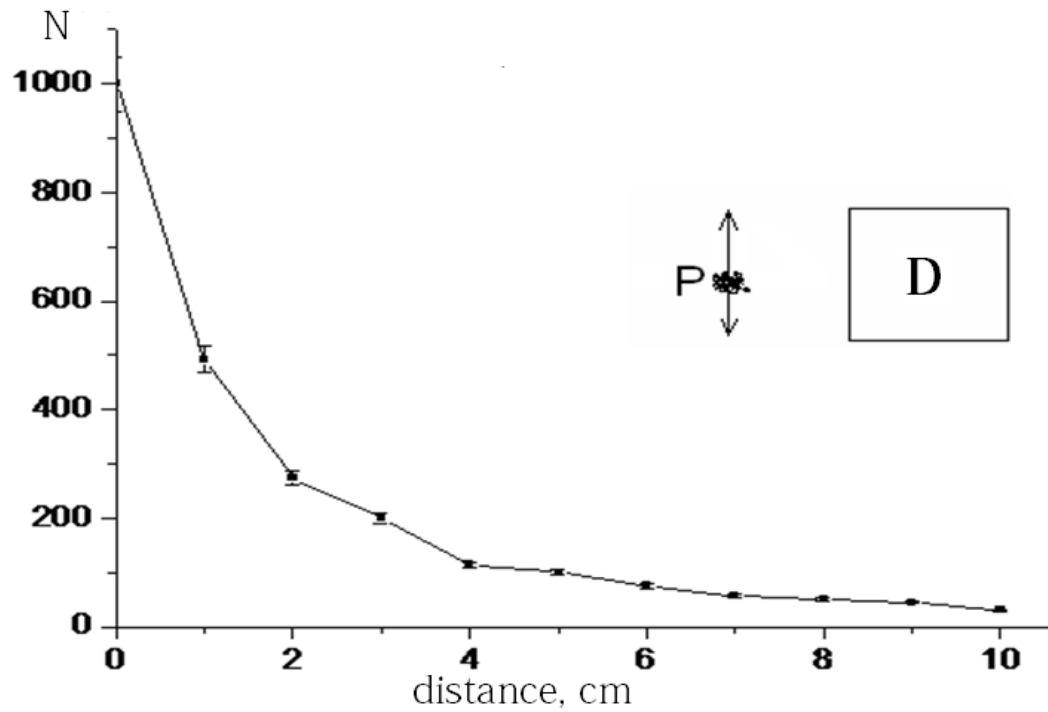


Fig.6. The counting rate dependence of the  $\gamma$  - source ( $^{137}\text{Cs}$ ) displacement from the center of the detector.



## Conclusions :

Scintillator replacement on  $\text{LaBr}_3:\text{Ce}$  and using SiPM of HAMAMATSU firm allowed to improve the energetic resolution for  $\gamma$ -locator from 22% to 8%.

Source  $^{137}\text{Cs}$  (662keV) ER=8% for  $\text{LaBr}_3:\text{Ce}$  scintillator and Source  $^{137}\text{Cs}$  (662keV) ER=13% LYSO scintillator.

Source  $^{241}\text{Am}$  (60keV) ER=28% for  $\text{LaBr}_3:\text{Ce}$  scintillator and Source  $^{241}\text{Am}$  (60keV) ER=44% LYSO scintillator.

Experimental data show that the noise level is much lower than the instruments useful signal. Signal / background (noise) ratio  $\sim 1000$ .

This research results achieved using sources with the activity much lesser than the ninety nine Technetium activity used in clinical practice. It is hoped that the signal / background ratio is much higher when dealing with the real short half-life source.

Thanks for you time.